Magnetic Resonance Imaging of Structure, Diffusivity, and Copper Immobilization in a Phototrophic Biofilm

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Magnetic resonance imaging (MRI) was used to spatially resolve the structure, water diffusion, and copper transport of a phototrophic biofilm and its fate. MRI was able to resolve considerable structural heterogeneity, ranging from classical laminations ~500 μm thick to structures with no apparent ordering. Pulsed-field gradient (PFG) analysis spatially resolved water diffusion coefficients which exhibited relatively little or no attenuation (diffusion coefficients ranged from $1.7 \times 10^{-9}$ m² s⁻¹ to $2.2 \times 10^{-9}$ m² s⁻¹). The biofilm was then reacted with a 10-mg liter⁻¹ Cu²⁺ solution, and transverse-parameter maps were used to spatially and temporally map copper immobilization within the biofilm. Significantly, a calibration protocol similar to that used in biomedical research successfully quantified copper concentrations throughout the biofilm. Variations in Cu concentrations were controlled by the biofilm structure. Copper immobilization was most rapid (~5 mg Cu liter⁻¹ h⁻¹) over the first 20 to 30 h and then much slower for the remaining 60 h of the experiment. The transport of metal within the biofilm is controlled by both diffusion and immobilization. This was explored using a Bartlett and Gardner model which examined both diffusion and adsorption through a hypothetical film exhibiting properties similar to those of the phototrophic biofilm. Higher adsorption constants (K) resulted in longer lag times until the onset of immobilization at depth but higher actual adsorption rates. MRI and reaction transport models are versatile tools which can significantly improve our understanding of heavy metal immobilization in naturally occurring biofilms.

The biofilm is an exceptionally common mode of life for bacteria in natural, clinical, and engineered environments. These microbial “cities” range in thickness from a few cells to several centimeters and display a complex three-dimensional architecture which exhibits both structural and compositional heterogeneity (10, 22, 23).

Mass transfer rates within biofilms are controlled by diffusive and advective processes. Where interconnected pore spaces and channels exist within the biofilm, advection can play an important role in contaminant or nutrient mass transfer. In the cell clusters between channels or in biofilms where channels are absent, molecular diffusion becomes the dominant mass transfer mechanism (4, 21). Although the key transport medium within a biofilm is water, the molecular diffusion of a molecule through a biofilm is commonly slower than that in free water due to the lower permeability of the biofilm and the tortuous nature of any pathways. Consequently, the diffusion of nutrients (or indeed contaminants) can be rate-limiting in biofilm performance and can lead to steep chemical and redox gradients through the community (4, 6, 9, 17, 23). For that reason, direct measurements of biofilm diffusion properties are highly desirable when modeling biofilm function (3, 40). Biofilms, however, are complex structures which exhibit a high degree of structural and compositional heterogeneity. Consequently, mass transfer rates can also display a high degree of heterogeneity. Protocols which can map these heterogeneities throughout the biofilm aid the effective modeling of biofilm operation (3, 40).

Quantifying the transport and determining the fate of heavy metals in aqueous systems are integral to understanding, predicting, and preventing heavy metal contamination in the natural environment. Bacteria have tremendous potential to influence the transport and fate of metals through the complexation of metals to the bacterial surface and via metabolic processes (18, 19, 32). The ability of bacteria to absorb large quantities of metal ions to their surfaces results from the abundance of ionizable carboxyl and phosphoryl groups within the cell wall, which behave as metal-reactive ligands (19, 28, 42). Furthermore, bacterial metabolism can dramatically impact metal mobility, either via direct metabolic oxidation or reduction of the metal or via mobilization or immobilization of sister phases, which results in heavy metal release or capture (18, 26). The ubiquitous nature of bacteria in almost any natural environment where there is sufficient water for their survival ensures that they are key players in the cycling of heavy metals.

In biofilms, mass transport must play a key role in controlling the rate of metal sequestration. That is, metal ions must diffuse (and advect) through the matrix of cells and extracellular polymers; the rate at which this occurs mediates the rate at which the biofilm immobilizes that metal. This contrasts with planktonic systems, which are not subjected to the diffusion limitation experienced by biofilms and thus may exhibit more rapid reaction kinetics. Thus, quantifying both the mass transport and the immobilization of a metal is essential to our understanding of biofilm metal sequestration. To date, metal uptake in biofilms has been quantified from bulk measurements, commonly of the total metal retained within the biofilm.

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(see, e.g., references 15 and 27). Although informative, these studies do not reveal the spatially resolved and cross-correlatable information on metal immobilization, diffusivity, and biofilm structure required to fully understand the mass transfer and fate of metal in biofilms. Significantly, magnetic resonance imaging (MRI) has the potential to do this.

MRI has been widely applied to the study of both porous media and mass transport phenomena. The ability to study structure, diffusion, flow, molecular dynamics, and chemical reactions noninvasively has been widely utilized in fields such as medicine (38), separation science, food science, physical science (7), rheology (24), and chemical engineering (14). Its particular suitability to the study of porous media has led to its application to biofilm research. For example, pulsed-field gradient (PFG)–nuclear magnetic resonance (NMR) has been used to determine water diffusion rates in biofilms (20, 39), while the molecule-specific sensitivity of NMR has enabled researchers to map depth-dependent metabolite profiles (25).

Heavy metal precipitation has also been imaged temporally and spatially in bioreactors containing polyurethane-immobilized biofilms (30, 31). MRI is a particularly suitable technique for biofilm research, as it is a noninvasive approach which allows analysis in vivo, in situ, and in three dimensions.

The key aim of this study was to investigate the ability of MRI to characterize the transport and fate of heavy metal in a natural biofilm, thus demonstrating its potential for probing biofilm-metal interactions in natural systems. This initial study utilized a 1-cm-thick phototrophic biofilm from an Icelandic hot spring as a “model” biofilm. This biofilm was considered ideal for the current study because it is structurally complex, enabling us to investigate the ability of MRI to map and correlate the diffusivity in, heavy metal uptake in, and structure of a complex biofilm system. Copper was chosen as an ideal metal for study because it is a common heavy metal pollutant and because it is sufficiently paramagnetic to be readily detectable by 1H-MRI.

In this study, we utilize MRI to shed light on biofilm heavy metal immobilization by quantifying the structure, diffusivity, and copper transport of a biofilm and its fate in three dimensions and in real time. This is the first study combining biofilm structure, diffusivity, and metal immobilization. This study also for the first time applies a calibration protocol which directly quantifies metal concentrations inside a biofilm.

**MATERIALS AND METHODS**

Biofilm. The natural biofilm used in this study was a 1-cm-thick phototrophic biofilm, collected in September 2005 from the southwestern discharge channel of the Strokkur Geyser, Geysir hot spring system, southern Iceland (latitude +64°18′40″, longitude −20°18′10″).

Flow system. The biofilm was positioned in a 1.5-cm-diameter plastic reaction cell by fixing it into a bed of agar (Fig. 1). The biofilm was positioned in the agar so that the lower portion was surrounded by agar, reflecting the fact that in the natural environment the lower portion is laterally continuous, connecting to other biofilms; only the upper portion stands free in the spring water. The reaction cell containing the biofilm was then positioned in the center of the magnet. The reaction cell remained in position inside the magnet for the 60-h duration of the experiment. The reaction cell containing the biofilm was first connected via silicon tubing to an 18 MΩ water supply and slowly washed with ultrapure water. The system was then connected to a 4-liter reservoir of a 10-mg liter−1 Cu²⁺ solution prepared using CuSO₄ • 5H₂O. A peristaltic pump was used to pump the solution through the reactor tube at a rate of 0.7 ml/min. The Cu solution eluent was pumped back into the reservoir.

MRI measurements were of 14 contiguous slices, perpendicular to flow. (B) For each slice, 64 $T_2$-weighted images are acquired with increasing echo time. (C) For each pixel, the decay of the MRI signal can be fitted to an exponential function, giving a $T_2$ value. Taking the $T_2$ values for each pixel yields a $T_2$ parameter map. The approximate scale (height) of a biofilm is 1 cm. Relative dimensions are not exact.

**FIG. 1.** (A) Reaction cell with the biofilm held in place by agar. MRI measurements were of 14 contiguous slices, perpendicular to flow. (B) For each slice, 64 $T_2$-weighted images are acquired with increasing echo time. (C) For each pixel, the decay of the MRI signal can be fitted to an exponential function, giving a $T_2$ value. Taking the $T_2$ values for each pixel yields a $T_2$ parameter map. The approximate scale (height) of a biofilm is 1 cm. Relative dimensions are not exact.

MRI. The basic principles of 1H-based MRI (the type of MRI used in this study) are as follows. The hydrogen nucleus possesses both a magnetic moment and spin-angular momentum, commonly referred to as a nuclear “spin.” There is a slight tendency for these nuclear spins to align with the direction of an applied magnetic field, $B_0$, thus creating a net magnetization in the sample. The nuclear spins precess about the axis of the applied magnetic field, $B_0$, at a frequency of $γB_0$, where $γ$ is the magnetogyric ratio. The spins can be manipulated by the application of electromagnetic radiation that matches this precession frequency (i.e., radio frequency [RF]). Following excitation by this RF pulse, the spins return to equilibrium; this process is called relaxation. $T_2$ relaxation, the transverse-relaxation time of hydrogen nuclei within water molecules, describes the process whereby spins lose phase coherence, and $T_1$ (longitudinal) relaxation describes the process whereby the net magnetization returns to equilibrium.

Imaging is achieved by application of linear magnetic field gradients across the sample, causing spins at different spatial positions to experience slightly different magnetic fields and hence to precess at different frequencies, thus labeling their spatial positions. This enables the $T_2$ or $T_1$ relaxation at each position to be mapped. In simple terms, $T_2$ relaxation is detected by the RF coil which surrounds the sample (in this study, it is the same coil as that which emits the original RF pulse). The resolution of the image is dependent on the diameter of this RF coil, with smaller coils resulting in higher-resolution images. Very small diameter coils (e.g., 4 mm) can achieve a resolution of a few 10s of micrometers.

The MRI experiments were performed on a Bruker Avance BioSpec system, using a 30-cm-bore, 7T superconducting magnet (Bruker BioSpec, Karlsruhe, Germany). A Bruker microimaging gradient insert (model BG-6) and 100-A gradient amplifiers provide strong linear magnetic field gradient pulses of up to 1,000 mT/m, thus allowing the system to adapt to perform microimaging experiments. A Bruker 35-mm-diameter birdcage RF volume resonator was used to excite and detect the 1H signal.

MRI imaging was used to measure $T_2$. The $T_2$ value at different biofilm loca-
Henkelman (36) found that the copper concentrations (ranging from 0 to 4,000 mg liter\(^{-1}\)) was investigated. Several types of media with different solids contents (i.e., water, agar, bacterial pellet, agar-bacterium composite, and agar-cyanobacterium composite) were used for basic structural imaging of the biofilm. From these, \(T_2\) parameter maps were calculated (Fig. 1). In the \(T_2\) parameter maps, the image intensity is the actual \(T_2\) value. These parameter maps were used to obtain quantitative images of copper concentration.

**Acquisition of \(T_2\)-weighted images.** \(T_2\)-weighted images were obtained using a multislice, multispin echo, two-dimensional imaging sequence; 64 consecutive thickness of 1 mm. The field of view was 26 by 26 mm, using an imaging matrix of 130 by 130 pixels, giving an in-plane resolution of 200 by 200 \(\mu\)m. Two signal averages were taken, giving a total imaging time of 30 min.

**Calculation of \(T_2\) parameter maps.** \(T_2\) parameter maps were calculated from the series of \(T_2\)-weighted images for each slice (Fig. 1B and C) by fitting the signal decay for each individual pixel to an exponential function:

\[
S(t) = S(0)e^{-T_2/B} + B
\]

where \(S(0)\) is the MRI signal at time 0, \(S(t)\) is the MRI signal at time \(t\), \(B\) is a baseline offset parameter, and \(T_2\) is the decay constant for the transverse relaxation of the MRI signal back to equilibrium. It was found that all the signal decay curves were well fitted by such a single exponential function. The presence of paramagnetic metals, such as copper, can cause a reduction in \(T_2\). Consequently, construction of \(T_2\) parameter maps during copper uptake can be used to reveal the location and relative concentration of copper.

**Calibration of copper concentrations from \(T_2\) parameter maps.** Significantly, this qualitative assessment can be calibrated to gain quantitative values for copper concentrations throughout the biofilm. The effect of paramagnetic ions, such as Cu\(^{2+}\), on the relaxation times of pure water was first considered theoretically by Bloembergen (5) with the equation:

\[
[S] = \frac{1}{R} \left( \frac{1}{T_2} - \frac{1}{T_2,0} \right)
\]

where \(T_2,0\) is the relaxation time in the absence of ions, \(T_2\) is the relaxation time in the presence of ions, \([S]\) denotes the concentration of the copper ions, and \(R\) is the relaxivity constant of the ions. \(R\) describes how the concentration of paramagnetic ions changes the \(T_2\) relaxation time. In the current study, \(T_2,0\) and \(T_2,0\) are known variables, as they are taken directly from \(T_2\) parameter maps. \(R\), however, is unknown and must be separately determined to enable the calculation of \([S]\). In similar human MRI studies where the concentration of gadolinium (Gd) paramagnetic contrast agents were measured, it has been common practice to assume that \(R\) is independent of tissue environment and simply to use a value for water. For example, a recent study has described how the relaxivity of the MR signal for many MR contrast agents increases linearly with the concentration of agent. The 

**Light microscopy.** Following MRI analysis, the biofilm was sectioned into 2-mm slices with a sterile scalpel and fixed in a solution of 2.5% glutaraldehyde with 0.05 M HEPES, pH 7, for 24 h. Tissue was then dehydrated through graded ethanol concentrations (70%, 90%, and 100% ethanol [four times], 24 h each), imbedded in LR White (hard) resin, and sectioned on an ultramicrotome. Thin sections were viewed on a Zeiss Axioplan microscope with a Nikon DN100 digital camera.

**Bulk copper analysis by AAS.** After reaction with copper, two sections of the biofilm were retained and measured to determine volume. These were then placed in 0.5 ml concentrated HCl, disaggregated, and incubated at room temperature for 24 h to disperse the immobilized copper. This material was then spun down to pellet the organic material, and the eluent was transferred to 10 ml ultrapure water and analyzed for Cu by AAS.

**Modeling of coupled diffusion-adsorption within a model biofilm.** The coupled diffusion-adsorption process has been considered previously for thin films by Bartlett and Gardner (1). Adsorption of the adsorbate, \(A\) (e.g., Cu\(^{2+}\)), onto a binding site, \(S\), can be described with the following simple reversible reaction:

\[
A + S \rightleftharpoons AS
\]

with the equilibrium constant (referred to herein as the adsorption constant), \(K\), equal to

\[
K = k_s/k_a = [AS]/[A][S]
\]

where \(k_s\) and \(k_a\) are the forward and backward rate constants. By assuming no interaction between adsorbed molecules, the adsorption process can be described by the Langmuir isotherm. For the one-dimensional case, taking \(s\) as the distance into a film of thickness \(L\), \(t\) as time, and \(b\) as the fraction of sites occupied (at a specified distance and time), the diffusion reaction equation for adsorbate \(A\) is given by

\[
D \frac{\partial^2 A}{\partial x^2} = k_s(A - 1)N + k_aDN = \frac{\partial A}{\partial t}
\]

where \(D\) is the diffusion coefficient, \(N\) is the concentration of the binding sites within the film, \(a\) is the concentration of diffusing species \(A\) (at a specified distance and time) within the film, and \(a_a\) is the constant concentration main-
tained at the top boundary of the film. Consideration of the kinetics at the reaction sites gives

\[ N \frac{\partial \theta}{\partial t} = k_{a}(1 - \theta) - k_{d} \theta N \]  

(6)

Equations 5 and 6 are coupled nonlinear partial differential equations that do not have an exact analytical solution. However, Bartlett and Gardner (1) found that the problem could be divided into six cases and presented the approximate analytical solutions for each case. They introduced the following dimensionless parameters: \( \chi = \frac{x}{L} \), \( \tau = D L^{2} \), \( \eta = k_{N} L^{2} D \), \( \lambda = k_{o} \), and \( \eta = \frac{1}{\lambda} \), giving the following coupled nonlinear partial differential equations:

\[ \frac{\partial \chi}{\partial \tau} - \frac{\chi}{\lambda} \frac{\partial \chi}{\partial \tau} = \eta \frac{\partial \theta}{\partial \tau} \]  

(7)

\[ \eta \frac{\partial \theta}{\partial \tau} = \lambda \eta (1 - \theta) - k_{o} \theta \]  

(8)

For a film with slow diffusion, where equilibrium is maintained between the diffusion species and the reactive sites and a large amount of absorbate is adsorbed by the sites (Bartlett and Gardner’s case 6 [1]), the solution involves a moving boundary, with position \( x_{m} \):

\[ (1 - \chi)^{2} = 1.5^{2} \frac{(x_{m} - x)^{2}}{\eta} \]  

(9)

The absorbate concentrations, on each side of the moving boundary, are given by \( \gamma_{1} \) and \( \gamma_{2} \):

\[ \gamma_{1} = \frac{\gamma_{m}}{\operatorname{erfc}(\eta \sqrt{1 - \chi})} + \operatorname{erf}(\chi \tau) \]  

(10)

\[ \gamma_{2} = 1 - \frac{1 - \gamma_{m}}{\operatorname{erfc}(\eta \sqrt{1 - \chi})} \]  

(11)

and the surface coverage is given by

\[ \theta = \frac{\lambda \gamma_{1}}{1 + \chi_{m}} \]  

(12)

To take account of the finite thickness of the film with an impermeable barrier, a correction term, \( \epsilon \), is applied.

\[ \epsilon(\chi, \tau) = \frac{\gamma_{m}}{\operatorname{erfc}(\eta \sqrt{1 - \chi})} \left[ \operatorname{erfc}(\frac{1 - \gamma_{m}}{2 \tau}) - \operatorname{erf}(\frac{\gamma_{m} - \chi_{m}}{2 \tau}) \right] \]  

(13)

Based on results from MRI analysis, variables representative of the phototrophic biofilm were put into the model. Details of these variables are provided in Results and Discussion but are also summarized here for clarity. For this example, a best-case scenario with the highest relative diffusion coefficient (\( D_{p} \)) (1.0) and pore volume fraction (\( \phi \)) (0.9) was chosen, generating a relative effective diffusivity (\( D_{rel} \)) of 0.9 (see Results and equations 15 and 16 for details). Quick-enden and Xu (33) reported the diffusion coefficient for Cu \(^{2+} \) in an infinitely dilute solution at 25°C to be \( 7.8 \times 10^{-10} \) m \(^2\) s \(^{-1}\). Multiplying this value by \( D_{rel} \), which has no apparent systematic pattern (Fig. 2A, D, E, F, K, and L). In slices E to H, the biofilm appears to be composed of two adjacent structures. This is most clearly defined in slices G and H, which exhibit a well-defined, narrow, central divide separating the two sections. The fact that this septum is dark (i.e., exhibits a low \( T_{2} \) value) indicates that the divide is composed of dense, low-water-content material and is not filled with water. The two adjacent structures merge, eventually forming one continuous structure in Fig. 2F. The brightest regions exhibit the same \( T_{2} \) value as water, indicating that these features are large, water-filled channels or pores (exemplified in Fig. 2B, D, E, and F). These features, however, are quite rare. Conversely, dark regions of low \( T_{2} \) relaxation are common in all slices and are particularly abundant at the base and sometimes the sides of the biofilm. These regions of very low \( T_{2} \) relaxation must result either from the presence of very high density organic matter (which is due to the fact that its lower water content reduces \( T_{2} \)) or from the presence of mineral particulates (which reduce \( T_{2} \) either by reducing water content or by introducing paramagnetic atoms into the system). Simple visual inspection of the biofilm reveals that the very low \( T_{2} \) regions at the base of the biofilm are due to a high concentration of mineral particulates.

Light microscopy of thin sections and unprocessed biofilm revealed that the biofilm was dominated by the filamentous cyanobacterium Phormidium sp. throughout. Within the biofilm, the main structural heterogeneities result from variations in the packing density of this organism (Fig. 3).

**Bioluminescence imaging.** Analysis of the impact of solids content on copper relativity, \( R \), shows that \( R \) increases linearly with solids content (Fig. 5). A linear least squares fit to the data in Fig. 1 gives

\[ R = 0.001845S + 0.01142 \]  

(14)

where \( S \) is the percent solids content of the media. The solids content of the biofilm was determined to be 9.8%, and this

**RESULTS**

**MRI of a biofilm structure.** Prior to the injection of copper solution, \( T_{2} \)-weighted images were collected for 14 consecutive slices through the biofilm. For each slice, 64 images were acquired, each with a longer echo time and greater \( T_{2} \) weighting. This allowed selection of the echo time (\( T_{2} \) weighting) which best revealed structural detail. Figure 2, which shows the 14 slices at an echo time of 101 ms, reveals the considerable structural complexity of the biofilm. Particularly striking is the layered substructure apparent in many of the slices (exemplified in Fig. 2F but also present in Fig. 2B, C, G, and H). These layers are commonly curved (convex side up) into a conformic architecture. Lamina-

\[ T \]
value was put into equation 14, generating an $R$ value of 0.0295 s$^{-1}$ mg$^{-1}$ liter$^{-1}$. This $R$ value was used in equation 2, enabling calculation of the copper concentration from the $T_2$ parameter maps.

**Dynamic Cu immobilization within the biofilm.** The biofilm was then challenged with a 10-mg/liter Cu$^{2+}$ solution for 60 h, and the MRI was used to quantitatively image the Cu concentration within the biofilm. Figure 6 depicts a series of maps showing copper concentrations throughout a biofilm slice (the same slice as in Fig. 2J) after 6, 12, 18, 24, and 60 h of reaction with copper. It should be noted here that during the 60-h reaction with the copper solution, the very top 2 mm of the biofilm exhibited significant positional shift that could not be overcome by registration of the $T_{2i}$ maps onto the reference $T_{2,0}$ map. This prevented a reliable calculation of the copper concentration in this very top zone; hence, we do not show results for the top 2 mm. Copper immobilization was most rapid over the first 24 h and then increased very slowly for the remainder of the experiment. This is shown by the notable brightening of the images from 6 to 24 h (Fig. 6A through D), followed by a smaller increase in brightness between 24 and 60 h (Fig. 6D to E). The rate and amount of copper immobilization were heterogeneous throughout the biofilm. For example, after the first 6 h, some regions, in particular the lower central portion of the biofilm, had failed to accumulate any copper, while other areas displayed significant copper uptake (Fig. 6A). Where the biofilm exhibited a layered structure, the copper was immobilized into alternating layers of high and low copper concentrations, which reflected this structure.

Copper immobilization reached a maximum of $\sim$90 mg Cu per liter of biofilm (Fig. 7A) (note that all copper concentrations in the biofilm are reported as mg Cu per liter volume of biofilm). A 10- to 30-mg liter$^{-1}$ difference in copper concentration occurred between the alternating layers of high and low copper concentrations (Fig. 7A). Copper uptake profiles confirmed that Cu immobilization was most rapid over the initial $\sim$20 to 30 h, with an uptake rate of $\sim$5 mg liter$^{-1}$ h$^{-1}$ at its most rapid (Fig. 7A and B). In general, Cu immobilization rates over this initial period were slower with increasing depth into the biofilm. Cu immobilization rates then notably slowed for the later part (h 30 to 60) of the experiment (with rates commonly around 0.3 mg liter$^{-1}$ h$^{-1}$). One exception to this was the uptake rate at 7.5 mm, which did not notably slow during this later period.

Significantly, the accuracy of the MRI Cu calibration was strongly supported by AAS analysis of the acid-digested biofilm material. AAS analysis recorded that the biofilm exhibited a bulk copper concentration of 59.5 and 63.6 mg liter$^{-1}$ Cu from the two
samples analyzed. Similarly, the bulk average copper density in the biofilm determined by MRI was 60 mg liter$^{-1}$.

A Bartlett-Gardner model was used to explore diffusion adsorption phenomena in a hypothetical film with properties similar to those of the phototrophic biofilm studied here. Depth-dependent concentration-time plots generated using this model are shown in Fig. 8. For an adsorption constant of $2 \times 10^4$, initial adsorption rate decreases with depth and there is a short lag time until the onset of Cu adsorption deeper within the film (Fig. 8). At increasing values of $K$, the lag time until onset of adsorption increases, and the initial absorption rate also increases. At the highest $K$ value ($1.5 \times 10^5$), the onset of the adsorption lag time now dominates the uptake profile (Fig. 8).

**DISCUSSION**

MRI was very successful in revealing complex structural heterogeneity within the natural biofilm. Within the ~1-cm$^3$ biofilm volume, considerable variations in structure ranging from a highly ordered coniform layering to complex structures with no apparent organization were observed. Layered structures are a common feature of phototrophic biofilms (8, 34), resulting from differing cellular densities, orientations, and taxa. Large variations in taxonomic composition within phototrophic biofilms commonly result in distinct bands differentiated by marked color differences. However, simple visual inspection revealed that the biofilm was very light green throughout and, except for a distinct 1-mm dark green layer at the very top of the biofilm, only very faint structural features, such as coniform laminations, could be observed. Light micros-

FIG. 3. Light micrographs of thin biofilm sections showing zones of high-density (a) and low-density (b) filament packing. Scale, 50 μm.

FIG. 4. Examples of a water diffusion map and profiles. (A) MR slice showing the biofilm structure (the area taken from the slice shown in Fig. 2J). (B) Corresponding relative water diffusion coefficient map. The differences in contrast reflect differences in water diffusion coefficients. (C) Profile of actual water diffusion coefficients along the transect shown in panels A and B. Overall, little variation in the water diffusion coefficient was observed. The scale of the line of transects in panels A and B is 7.5 mm long.

copy of thin sections and unprocessed biofilm revealed that the main structural heterogeneities resulted from variations in the packing densities of the cyanobacterium Phormidium sp., which dominated the biofilm.

Normal visual and light microscopy also confirmed that the very dark areas around the base of the biofilm and in the divide
between the two sections (Fig. 2) contained high concentrations of mineral material. The base is a mix of mineral and microbial components, where microbes grew among the mineral particulates much like in a stromatolite. Eventually, however, biofilm growth would have exceeded the mineral accumulation rate, leading to the growth of the rest of the biofilm with minimal mineral acquisition.

Some water-filled pores are observed in Fig. 2. These are, however, rare and appear to be individual entities (i.e., pore spaces rather than connected channels). Evidently, the biofilm lacks significant interconnected large-scale channels which would act as major nutrient and gas transport pathways under flow conditions. Although channels could exist below image resolution, the rarity of channels was further corroborated by light microscopy of thin sections. Consequently, diffusive transport processes must dominate within this biofilm.

Evaluation of water diffusivity is pertinent because water is the key medium in which other essential compounds, such as nutrients and waste, are dissolved. Studies which record diffusion coefficients for water along with other molecules in biofilms show an exceptionally close relationship between the diffusivity of water and the diffusion coefficients of the other measured molecules (2, 11, 12, 39), indicating that water diffusivity can be used to estimate the diffusion of other essential compounds (2, 40). PFG analysis offers a rapid technique for evaluating water diffusion. This approach, however, has traditionally reported only bulk average diffusion coefficients for the entire biofilm and thus does not reveal spatial-diffusion heterogeneities resulting from biofilm complexity. In response to this, Wieland et al. (40) advanced the PFG approach to spatially map water diffusion coefficients through a phototrophic biofilm. We utilize the same approach here. In the current study, water diffusion coefficients showed little or no attenuation throughout the biofilm, with water diffusion coefficients most commonly being between the unattenuated value $2.2 \times 10^{-9}$ m$^{-2}$ s$^{-1}$ ($D_r = 1.0$) and $1.9 \times 10^{-9}$ m$^{-2}$ s$^{-1}$ ($D_r = 0.86$), although they dropped as low as $1.7 \times 10^{-9}$ m$^{-2}$ s$^{-1}$ ($D_r = 0.77$) (the relative diffusion coefficient, $D_r$, is the diffusion coefficient normalized to the unattenuated diffusion coefficient in free water). Notably, there appears to be relatively little diffusion heterogeneity, considering the structural complexity of the biofilm. PFG analysis determined that values for $D_r$ for the phototrophic biofilm studied by Wieland et al. (40) varied between 0.4 and 0.9 and thus showed zones with higher diffusion attenuation and greater diffusion heterogeneity than those of the phototrophic biofilm studied here. The two key factors which control diffusivity are the packing density of cells and extracellular polymeric substances (EPS); an increase in the volume fraction of these components causes a decrease in the diffusion coefficient (2). Cellular and EPS material reduce diffusivity by acting as solid obstructions which increase the tortuosity of the diffusive path length. In this study, however, the volume fraction of cellular and EPS material was evidently sufficient to cause only limited diffusion attenuation. Compared to the cell volume fraction, the EPS volume fraction is considered to have a greater impact on diffusion rates (2, 16). Staining of thin sections with 1% toluidine blue–1% borax revealed an abundance of EPS material filling the spaces between bacteria and forming the matrix of the biofilm. Cellular volume fraction varied from almost 0 to approximately 30%; the biofilm is dominated by an extracellular matrix (30–70 to 100%) (determined by area analysis of thin sections using ImageJ software). Despite its relative abundance, the EPS in this case failed to cause notable water diffusion attenuation. EPS and cellular material also affect mass transport processes by reducing the pore volume available for diffusion. Thus, the amount of a substance transported is controlled by both its rate of diffusion and the volume available for it to diffuse through. Considering the fact that the pore volume fraction generates the value $D_{eff}$.

$$D_{eff} = D_r \Phi$$

where $\Phi$ is the pore volume fraction and $D_{eff}$ is the relative effective diffusivity. Void fraction can be estimated from the dry density of the biofilm using the equation

$$1 - \left( \frac{B_v}{\rho} \right) e_v + \left( \frac{B_s}{\rho} \right) e_s = \Phi$$

where $B_{vj}$ is the biofilm dry mass per hydrated volume of

**FIG. 5.** Impact of solids content on copper Cu relaxivity. Media used were water (U), agar (V), agar-cyanobacteria (W), 30:60 bacteria-agar (X), 50:50 bacteria-agar (Y), and the bacterial pellet (Z). Standard deviations were relatively small, indicating that, at each solids density, $R$ remained consistent for a wide range of copper concentrations. Larger deviations in the 30:60 and 50:50 bacterium-agar media are probably due to the greater technical difficulty in the preparation of the standards.

**FIG. 6.** Quantitative copper concentration maps revealing copper immobilization in the biofilm after 6, 12, 18, 24, and 60 h (A, B, C, D and E, respectively). Brighter regions are regions of greater copper concentration. The grayscale indicates the copper concentrations (mg liter$^{-1}$). Scale (dashed line in panel E), 7.5 mm.
biofilm, \( \rho_c \) and \( \rho_e \) are cellular and EPS dry densities (per hydrated volume), respectively, and \( \epsilon_c \) and \( \epsilon_e \) are volume fractions of cells and EPS, respectively. Estimations of the void fraction typically apply values for \( \rho_c \) and \( \rho_e \) of \( \sim 0.35 \text{ g cm}^{-3} \) and \( 1.0 \text{ g cm}^{-3} \), respectively (37). Considering these parameters, the measured values for \( B_d \) of 0.1 g cm\(^{-3}\) and for \( \epsilon_c \) and \( \epsilon_e \) of 0.3 and 0.7 to 1.0, respectively, generate pore fractions between 0.84 and 0.9. While an estimate, this does suggest a relatively high pore fraction, resulting in only a small difference between \( D_e \) and \( D_{ce} \). Applying pore fraction values to equation 15 generates values for \( D_{ce} \) between 0.9 and 0.65. Although values of \( D_{ce} \) for some biofilm types can be as small as 0.07 (37), the \( D_{ce} \) values recorded here are consistent with those for phototrophic biofilms (35, 40).

In this study, MRI was successful in resolving copper immobilization throughout a phototrophic biofilm. Moreover, the application of a density-corrected calibration protocol enabled direct quantification of copper concentrations both temporally and spatially. Significantly, the copper concentration obtained from this calibration was supported by AAS analysis of biofilm digests. The biofilm immobilized an average of 60 mg Cu liter\(^{-1}\), with peaks of up to 90 mg liter\(^{-1}\), and Cu immobilization rates were most rapid over the first 20 to 30 h. In central, deeper zones of the biofilm, a lag time of \( \sim 6 \text{ h} \) occurred before the onset of copper immobilization. The copper immobilization rates observed within the biofilm are, in part, mediated by diffusion rates, which influence the rate of supply of Cu\(^{2+}\) throughout the biofilm. However, the transport of copper in the biofilm is controlled not only by diffusive processes but also by immobilization. As Cu\(^{2+}\) ions migrate through the film, some are immobilized, while others are free to diffuse further until they too are sequestered. The ratio of ions sequestered to those allowed to diffuse further is dependent on the immobilization constant (broadly speaking, the magnitude of the driving force behind immobilization). This could be the saturation index under supersaturated conditions (where precipitation may be the key immobilization mechanism) or the adsorption constant under undersaturated conditions (where adsorption onto cellular and EPS ligands is the key immobilization mechanism). Analysis of diffusion and copper immobilization not only enables quantification of these processes in real biofilms but also enables input of these parameters into reaction transport models for exploration of these phenomena further. To explore the adsorption scenario, a Bartlett and Gardner model which explicitly incorporates both diffusion and the reversible adsorption described by a one-site Langmuir isotherm (equations 3 to 13) (1) was used. The longer lag times until the onset of immobilization and the higher adsorption rates observed at higher \( K \) values (Fig. 8) reflect stronger adsorption by metal binding sites. That is, at higher \( K \) values, more of the copper ions are instantaneously adsorbed and further diffusion into the film is inhibited until these sites become close to saturated. At lower \( K \) values, more Cu\(^{2+}\) can diffuse through a given depth without being bound, leading to shorter lag times and lower initial adsorption rates.

Although this model is a simplified, homogeneous, one-dimensional version of a complex phototrophic biofilm, comparisons can be drawn between the model and the raw data. The rates of immobilization in the \( 2 \times 10^4 \) model are, broadly speaking, similar to those exhibited by the biofilm (compare Fig. 7B and 8A). The three models and the biofilm exhibit lag times until the onset of immobilization (although the lag times in the biofilm are shorter and, due to the time intervals of the experiment, apparent much deeper than in the models) (compare Fig. 7A and B and 8). There is also an approximate decrease in the initial rate of immobilization with depth in the biofilm (illustrated ideally in the models, particularly the \( 2 \times 10^4 \) model). It is notable that the adsorption rate at 7.5 mm did not notably slow during the experiment; this may be due to a much higher adsorption capacity at this location. In short, despite its complexity, key characteristics of combined adsorption-diffusion phenomena can be observed in the phototrophic biofilm.

Although we cannot rule out the possibility of precipitation as an immobilization mechanism here, if precipitation (driven by high pH) were the key immobilization mechanism, one would expect the metal to be rapidly and irreversibly immobilized upon entering the film. This process would bear greater similarity to systems with exceptionally high \( K \) values. Thus, in these systems, one would expect concentration-time curves
this study, one must expect considerably longer equilibration times in biofilms.

In this study, the experiments were performed in darkness and the biofilm was therefore not photosynthesizing. The obvious next step, then, is to examine the impact of photosynthesis (which raises the pH within the biofilm) on copper immobilization.

In this study we have shown that MRI is a valuable tool for quantifying (paramagnetic) heavy metal transport and determining the fate of heavy metals in naturally occurring biofilms. Significantly, copper concentrations can be directly calibrated using a solids-content-corrected calibration protocol. The ability of MRI to resolve both biofilm structure and diffusion coefficients enables the impact of these parameters on heavy metal transport and fate to be determined, thus revealing new insights into heavy metal-biofilm interactions in natural systems. Although in this study we focused upon Cu$^{2+}$, numerous other metals are sufficiently paramagnetic to be detected by MRI, including Ni$^{2+}$, Cr$^{3+}$, Co$^{2+}$, Ti$^{4+}$, Nd$^{3+}$, Th$^{4+}$, Fe$^{2+}$, and Mn$^{2+}$. Therefore, MRI has the potential to examine the transport and fate of a wide variety of potentially toxic (or indeed beneficial) metals in naturally occurring biofilms.

REFERENCES


